

On estimation of diffusion coefficient
based on spatio-temporal FRAP images:

An inverse ill-posed problem

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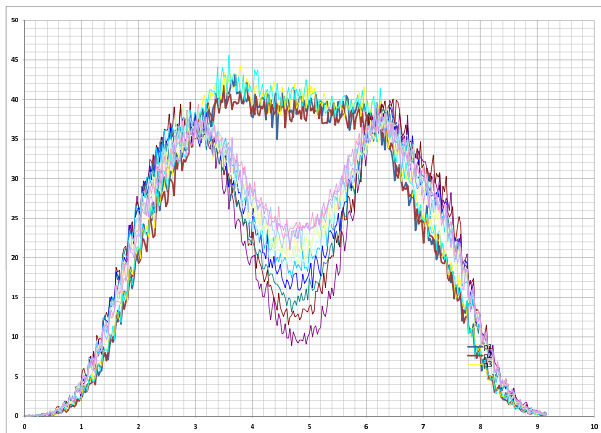
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PANM 16, 3. - 8. června 2012, Dolní Maxov

FRAP (Fluorescence Recovery After Photobleaching) technique allows detection of diffusivity of autofluorescence compound like proteins (e.g. phycobiliproteins) and also other non-fluorescence compound that are fluorescently tagged (e.g. green fluorescence proteins - GFP).

This method is based on application of short, intense laser irradiation (the so called bleach) to a small target region (Region Of Interest - ROI) of the cell that causes irreversible loss in fluorescence in this area without any damage in intracellular structures. After the "bleach" (or "bleaching"), the observed recovery in fluorescence in the "bleached area" reflects diffusion of fluorescence compounds from the area outside the bleach.

FRAP data: spatio-temporal image



Fluorescence intensity (in arbitrary units) vs. Distance [μm].
Experimental data from FRAP experiment with red algae *Porphyridium cruentum* describing the phycobilisomes mobility on thylakoid membrane.

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Our study describes the development and validation of a reliable method aiming to determine the phycobilisomes diffusivity on thylakoid membrane using FRAP experiments. This was usually done by experimental curve fitting to the analytical (closed form) models. For example, Moullineaux *et al.* (1997) have exploited the rotational symmetry of the cells by bleaching a plane across the short axis of the cell. Therefore, one-dimensional bleaching profiles along the long axis were generated.

C. W. Moullineaux supposed that:

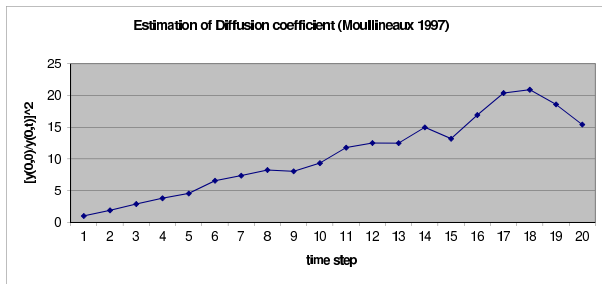
- 1 $x \in \mathbb{R}$, i.e. the infinite domain
- 2 the initial bleaching profile is Gaussian: $y(x, t_0) = y_{0,0} \exp \frac{-2x^2}{r_0^2}$, where r_0 is the half-width of the bleach at time $t_0 = 0$ and $\frac{y(x, t_0)}{y_{0,0}} = 1/e^2$ depth, $y_{0,0}$ is the maximum depth at time t_0 , i.e. the first post-bleach signal at the center ($x = 0$) subtracted from its pre-bleach level
- 3 boundary conditions correspond to the complete recovery: $y \rightarrow 0$ as $t \rightarrow \infty$, $y \rightarrow 0$ as $x \rightarrow \infty$.

C. W. Moullineux method

The calculation of the diffusion coefficient D according to Moullineux *et al.* resides in the weighted linear regression: a plot of $(\frac{y_{0,0}}{y(0,t)})^2$ against time, which should give a straight line with the tangent $\frac{8D}{r_0^2}$.

$$y(x, t) = \frac{y_{0,0}r_0}{\sqrt{r_0^2 + 8Dt}} \exp \frac{-2x^2}{r_0^2 + 8Dt}, \quad y(0, t) = \frac{y_{0,0}r_0}{\sqrt{r_0^2 + 8Dt}},$$

where $y(x, t)$ is the post-bleach signal at time t subtracted from the pre-bleach profile, $y(0, t)$ is the maximum depth at time t .



The **recovery** of unbleached particle concentration as a function of spatial coordinate r and time t is modeled with a linear, diffusion-reaction equation on a two-dimensional domain Ω :

$$\frac{\partial C}{\partial t} - \nabla \cdot (D \nabla C) = R(C) \quad (1)$$

- $C(r, t)$ is the unbleached particle **concentration**,
- D is the fluorescent particle **diffusivity** within the domain Ω (supposed to be a constant),
- $R(C)$ is a **reaction term**.

Reaction term $R(C)$ can be described as a first order reaction:

$$R(C) = -k_S C \quad (2)$$

- k_S is a **rate constant** describing bleaching during scanning.

- The **initial condition** is

$$C_0(r) = f(r, t_0) \quad \text{in } \Omega.$$

- The time varying **boundary condition** is
 - either of the **Dirichlet** type

$$C(r, t) = g(r, t) \quad \text{on } \partial\Omega \times [t_0, T],$$

- or of the **Neumann** type (based on the Fick's first law)

$$-D \nabla C(r, t) \cdot n(r) = h(r, t) \quad \text{on } \partial\Omega \times [t_0, T],$$

where $n(r)$ is the unit normal vector to $\partial\Omega$ inward Ω .

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Re-scaling to the dimensionless form

If we exploit the symmetry of our problem (according to Moullineux *et al.*), further adopt the form of reaction term according to (2) and introduce

- the dimensionless **spatial coordinate** $x \in [0, 1]$,
- the dimensionless **diffusion coefficient** $p > 0$,
- the dimensionless **time** $\tau \geq \tau_0$,
- the dimensionless normalized unbleached particle **concentration** y

by

$$x := \frac{r}{L}, \quad p := \frac{D}{D_0}, \quad \tau := t \frac{D_0}{L^2}, \quad y := \frac{C}{C_{pre}}, \quad (3)$$

where

- L is the **length of our specimen** in direction \perp to bleach spot,
- D_0 is a **constant** with some characteristic value (unit: m^2s^{-1}),
- C_{pre} is a **pre-bleach concentration** of C ,

we finally obtain the following form of **dimensionless diffusion-reaction equation** on one-dimensional domain, i.e. for $x \in [0, 1]$.

One-dimensional form of diffusion-reaction equation:

$$\frac{\partial y}{\partial \tau} - p \frac{\partial^2 y}{\partial x^2} = -\frac{k_S L^2}{D_0} y. \quad (4)$$

The **initial condition** is

$$y(x, \tau_0) = f(x), \quad x \in [0, 1]. \quad (5)$$

The time varying **boundary conditions** are either of the **Dirichlet** type

$$y(0, \tau) = g_0(\tau), \quad y(1, \tau) = g_1(\tau), \quad \tau \geq \tau_0, \quad (6)$$

or of the **Neumann** type

$$-p \frac{\partial y}{\partial x}(0, \tau) = h_0(\tau), \quad p \frac{\partial y}{\partial x}(1, \tau) = h_1(\tau), \quad \tau \geq \tau_0. \quad (7)$$

For the sake of clarity we further neglect the bleaching during scanning, i.e. we put $\frac{k_S L^2}{D_0} = 0$ (the right-hand side in (4) is zero).

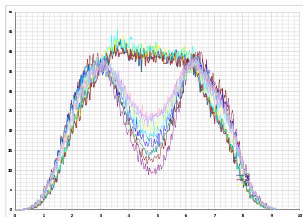
Experimental data

Based on FRAP experiments, we have a **2D dataset** in form of a table with $(N + 1)$ rows corresponding to the number of spatial points where the values are measured, and $(m + M + 1)$ columns with m **pre-bleach** and $M + 1$ **post-bleach** experimental values forming **1D profiles**

$$y_{exp}(x_i, \tau_j), \quad i = 0 \dots N, \quad j = -m \dots M.$$

In fact the process is determined by

- m columns of pre-bleach data containing the information about the steady state and optical distortion
- $M + 1$ columns of post-bleach data containing the information about the transport of unbleached particles (due to the diffusion) through the boundary



Experimental values:

- **space interval** between first and last measurement points: $[a, b]$
- **re-scaled dimensionless space interval**: $x \in [0, 1]$
- **length** of space interval: $L = b - a$
- **re-scaled distance** between two space measurements: $h = \frac{1}{N}$
- **time interval** between two measurements: T
- **re-scaled dimensionless time interval**: $\tau_t = \frac{TD_0}{L^2}$

Consequently,

$$x_0 = 0, \quad x_N = 1,$$

τ_0 corresponds to the first post-bleach measurement, and

- $y_{exp}(x_i, \tau_0)$, $i = 0 \dots N$, represents the IC,
- $y_{exp}(0, \tau_j)$, $j = 0 \dots M$, represents the left Dirichlet BC,
- $y_{exp}(1, \tau_j)$, $j = 0 \dots M$, represents the right Dirichlet BC,
- the Neumann BC for each j^{th} time instant is determined using the Fick's first law. This is possible thanks to the numerically computed **total flux $h(\tau_j)$** through the boundary. We suppose the symmetry, hence the total flux is equally divided into the left border ($x = 0$) and the right border ($x = 1$), see later for more details.

Recall that due to the measurement noise both the respective j – profiles $y_{exp}(x_i, \tau_j)$, $i = 0 \dots N$, and the initial and boundary conditions cannot be simply approximated by **a smooth function**. The forthcoming task is to analyze the measurement noise from real data and to treat it correctly.

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We construct an **objective function** J representing the **disparity between** the experimental and simulated time-varying concentration profiles, and then within a suitable method we look for such a value p **minimizing** J .

The usual form of an objective function is the **sum of squared differences** between the experimentally measured and numerically simulated time-varying concentration profiles:

$$J(p) = \sum_{j=0}^M \sum_{i=0}^N [y_{exp}(x_i, \tau_j) - y_{sim}(x_i, \tau_j, p)]^2, \quad (8)$$

where $y_{sim}(x_i, \tau_j, p)$ are the simulated values resulting from the solution of problem (4)–(6).

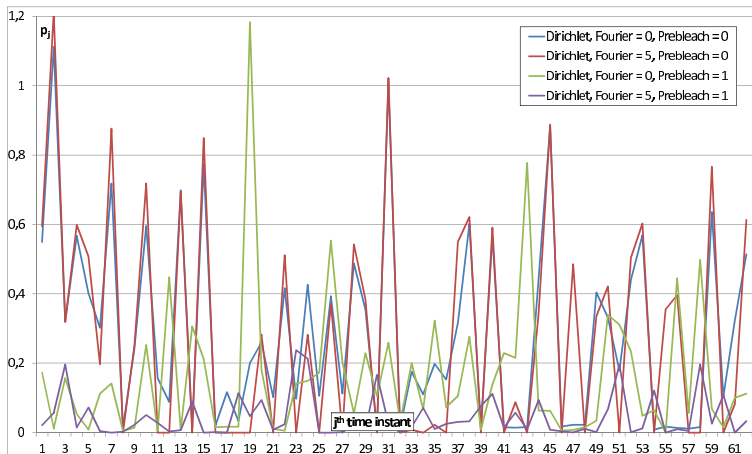
Taking into account the biological reality residing in possible time dependence of phycobilins diffusivity, for the minimization problem

$$\min_p J(p) = \min_p \sum_{j=0}^M \sum_{i=0}^N [y_{exp}(x_i, \tau_j) - y_{sim}(x_i, \tau_j, p)]^2 \quad (9)$$

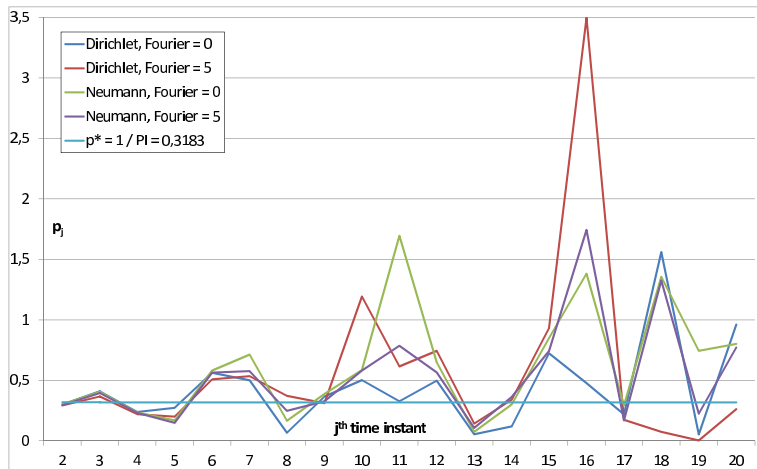
we further consider two cases:

- ① We can take both sums for i and j in (9) together. In this case, the scalar p is a result of minimization problem for J .
- ② We can consider each j^{th} time instant separately. In this case, the M solutions $p_1 \dots p_M$ correspond to each minimization problem for fixed j in sum (9) and we can observe a 'dynamics' of diffusion coefficient p_j evolution.

Data *P. Cruentum* - 11-11 14: diffusion coefficients p_j



Test data: diffusion coefficients p_j



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We assume model in form of

$$T(p) = f$$

and we want to find

$$p = T^{-1}(f).$$

Operator T is not analytically invertible, therefore we want to find

$$p^* = \arg \min_p \|T(p) - f\|^2.$$

In reality we have only approximation of $T - \tilde{T}$ and we don't have the exact data $- f = f_{\text{exact}} + f_{\text{noise}}$ and therefore we obtain

$$\tilde{p}^* = \arg \min_p \|\tilde{T}(p) - f_{\text{exact}} + f_{\text{noise}}\|^2.$$

Minimum of the functional \tilde{p}^* can be very far from exact p .

Example - backward heat equation 1

Let consider for simplicity we solve the heat equation with homogenous BC at $(-\infty, +\infty) \times (0, +\infty)$

$$\frac{\partial y}{\partial \tau} - p \frac{\partial^2 y}{\partial x^2} = 0$$

with initial condition

$$y(x, \tau_0) = f(x), \quad x \in (-\infty, +\infty). \quad (10)$$

Solution of this problem is

$$y(x, \tau) = (T(f)) = \int_{-\infty}^{\infty} K_{p\tau}(x-y)f(y)dy, \quad (11)$$

where $K_{\tau}(x) = \frac{1}{4\pi\tau} \exp(-\frac{x^2}{4\tau})$.

When we know the final state and searching IC, we solve the **Fredholm integral equation of first kind**. Operator T is compact, linear and its spectrum is discrete with cumulative point at 0.

Compact linear operators can be written in the form of **singular value expansion**

$$T(x) = \sum_{i=1}^{+\infty} \sigma_i \langle x, v_i \rangle u_i, \quad (12)$$

where u_i (v_i) are a complete orthonormal system of eigenvectors of TT^* (T^*T).

For some y we can find **pseudoinverse** T^\dagger of form

$$T^\dagger(y) = \sum_{i=1}^{+\infty} \frac{\langle y, u_i \rangle}{\sigma_i} v_i, \quad (13)$$

which satisfies $T^\dagger = (T|_{N(T)^\perp})^{-1}$.

Operator T^\dagger is unbounded. Noise in y can completely overlay the correct information.

Let $f \in C^1[0, 1]$ be any function, $\delta \in (0, 1)$, $n \in \mathbb{N}$ ($n \geq 2$) be arbitrary and define

$$f_n^\delta(x) := f(x) + \delta \sin \frac{n\pi x}{\delta}, \quad x \in [0, 1]. \quad (14)$$

Then

$$(f_n^\delta)'(x) := f'(x) + n \cos \frac{n\pi x}{\delta}, \quad x \in [0, 1]. \quad (15)$$

Now, in the uniform norm,

$$\|f - (f_n^\delta)\|_\infty = \delta, \quad (16)$$

but

$$\|f' - (f_n^\delta)'\|_\infty = n. \quad (17)$$

We can see, that the **derivative does not depend continuously on the data with respect to the uniform norm.**

From similar reasons our parameter identification problem

$$\tilde{p}^* = \arg \min_p \|\tilde{T}(p) - f_{exact} + f_{noise}\|^2$$

may not depend continuously on the data and may be very sensitive to noise f_{noise} .

Therefore we regularize the problem by adding the **regularization term**

$$\alpha \|p - p_{reg}\|^2.$$

We assume that $p(x, \tau)$ is almost constant with respect to x and τ and regularization term moves the minimum of functional \tilde{p}^* towards a constant function. In case $\alpha \rightarrow \infty$ we obtain $\tilde{p}^* = p_{reg}$.

We minimize new functional with respect to p and p_{reg}

$$\tilde{p}^* = \arg \min_{p, p_{reg}} (\|\tilde{T}(p) - f_{exact} + f_{noise}\|^2 + \alpha \|p - p_{reg}\|^2).$$

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Our problem is **ill-posed** in the sense that the solution, i.e. the diffusion coefficients

$$D_j = p_j D_0, \quad j = 1 \dots M$$

do not depend continuously on the initial experimental data. This led us to the necessity of using some stabilizing procedure:

- **Naive approach:** To remove the noise in experimental values, consider their smoothing by using the **Fourier transformation**.
- **Appropriate approach:** Formulation of **regularized cost functions**:

$$J_j(p, \alpha) = \sum_{i=0}^N [y_{exp}(x_i, \tau_j) - y_{sim}(x_i, \tau_j, p)]^2 + \alpha (p - p_{reg})^2 \quad (18)$$

for $j = 1 \dots M$, where $\alpha \geq 0$ is a regularization parameter, and p_{reg} is an expected value.

Taking $\alpha = 0$, function $J(p) = \sum_{j=0}^M J_j(p, 0)$ turns to (8).

Optimization problem

Minimizing J with respect to $p > 0$ represents a **one-dimensional optimization problem (OP)**. Three types of OP are considered:

- 1 Scalar p is a solution when taking both sums for i and j in together:

$$p^* = \arg \min_p \sum_{j=0}^M \sum_{i=0}^N [y_{exp}(x_i, \tau_j) - y_{sim}(x_i, \tau_j, p)]^2$$

- 2 Each j^{th} time instant separately without regularization ($\alpha = 0$)

$$p_j = \arg \min_p \sum_{i=0}^N [y_{exp}(x_i, \tau_j) - y_{sim}(x_i, \tau_j, p)]^2$$

- 3 Each j^{th} time instant separately using Tikhonov regularization

$$p_j(\alpha) = \arg \min_p \left\{ \sum_{i=0}^N [y_{exp}(x_i, \tau_j) - y_{sim}(x_i, \tau_j, p)]^2 + \alpha (p - p_{reg})^2 \right\}$$

We use a basic optimization method leading to values p^* , p_j , $p_j(\alpha)$ that minimize J . Values p_j , $p_j(\alpha)$ are approximations of diffusion coefficients.

Basic optimization method is an iteration process starting from an initial point $p^{(0)}$ and generating a sequence of iterates $p^{(1)}, p^{(2)}, \dots$ leading to a value p^* such that

$$p^{(l+1)} = p^{(l)} + \sigma^{(l)} d^{(l)},$$

where

- $d^{(l)}$ is a **direction vector** – is determined on the basis of values

$$p^{(j)}, J(p^{(j)}), J'(p^{(j)}), J''(p^{(j)}), \quad 0 \leq j \leq l,$$

- $\sigma^{(l)} > 0$ is a **step-length** – is determined on the basis of behavior of the function J in the neighborhood of $p^{(l)}$.

We use a suitable optimization method from the so-called UFO system

<http://www.cs.cas.cz/luksan/ufo.html>

In order to compute a function value $J_j(p^{(l)}, \alpha)$ in (18) for a given $p^{(l)}$ in the l^{th} iteration, we need to know both

- the **experimental** values $y_{exp}(x_i, \tau_j)$, $i = 0 \dots N$, $j = 0 \dots M$,
- the **simulated** values $y_{sim}(x_i, \tau_j, p^{(l)})$, $i = 0 \dots N$, $j = 0 \dots M$.

It means that in each l^{th} iteration we need to solve the problem (let put $y_{sim} \equiv y$, $p^{(l)} \equiv p$ for simplicity)

$$\frac{\partial y}{\partial \tau} - p \frac{\partial^2 y}{\partial x^2} = 0 \quad (19)$$

with the **initial and boundary conditions** defined by the experimental data:

$$y(x, \tau_0) = y_{exp}(x, \tau_0), \quad x \in [0, 1] \quad (20)$$

$$\text{(D)} \quad y(0, \tau) = y_{exp}(0, \tau), \quad y(1, \tau) = y_{exp}(1, \tau), \quad \tau \geq \tau_0 \quad (21)$$

$$\text{(N)} \quad -py'(0, \tau) = \frac{Flux(\tau)}{2}, \quad py'(1, \tau) = \frac{Flux(\tau)}{2}, \quad \tau \geq \tau_0 \quad (22)$$

Problem (19)-(22) for simulated data $y(x_i, \tau_j)$ was solved numerically using the **finite difference scheme** for uniformly distributed nodes with the space steplength Δh and the variable time steplength $\Delta \tau$:

- 1 The **explicit** scheme of order $\Delta \tau + \Delta h^2$:

$$y_{i,j} = \beta y_{i-1,j-1} + (1 - 2\beta)y_{i,j-1} + \beta y_{i+1,j-1}$$

- 2 The **Crank-Nicholson implicit** scheme of order $\Delta \tau^2 + \Delta h^2$:

$$-\frac{\beta}{2}y_{i-1,j} + (1+\beta)y_{i,j} - \frac{\beta}{2}y_{i+1,j} = \frac{\beta}{2}y_{i-1,j-1} + (1-\beta)y_{i,j-1} + \frac{\beta}{2}y_{i+1,j-1}$$

Here $\beta = \frac{\Delta \tau}{\Delta h^2} \rho$ and $y_{i,j} \equiv y(x_i, \tau_j)$ are the computed values in nodes that enter the function J as values $y_{sim}(x_i, \tau_j)$.

Recall that for the explicit scheme the condition $\beta \leq 1/2$ must hold.

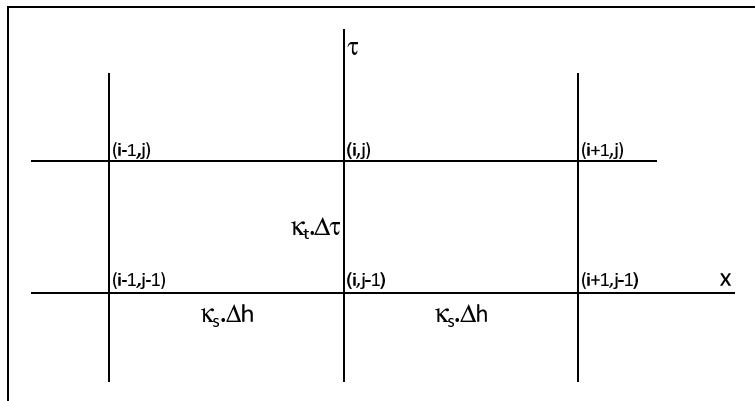
Steplengths used in the numerical scheme:

- **Space steplength:** $\Delta h = 1/N$ or $\Delta h = 1/(\kappa_s N)$, $\kappa_s \in \mathbb{N}$
- **Time steplength:** $\Delta \tau$ should be ideally of the same order as Δh^2 (or Δh in the CN scheme) and in the explicit scheme has to fulfill the relation $\Delta \tau \leq \frac{\Delta h^2}{2\rho}$.

In order to get from the $(j-1)^{th}$ time instant to the j^{th} , we need to perform

$$\kappa_t = \frac{TD_0}{L^2 \Delta \tau}$$

substeps, where $\kappa_t \in \mathbb{N}$ has to be an integer depending on $\Delta \tau$.



Neumann boundary conditions

When considering the Neumann BC, we use the following formulas:

$$-\frac{Flux(j)}{2p} = y'(0, \tau_j) = y'(x_0, \tau_j) \approx$$

1

$$\frac{y_{exp}(x_1, \tau_j) - y_{exp}(x_{-1}, \tau_j)}{2\Delta h}$$

2

$$\frac{-y_{exp}(x_2, \cdot) + 8y_{exp}(x_1, \cdot) - 8y_{exp}(x_{-1}, \cdot) + y_{exp}(x_{-2}, \cdot)}{12\Delta h}$$

3

$$\frac{-3y_{exp}(x_4) + 16y_{exp}(x_3) - 36y_{exp}(x_2) + 48y_{exp}(x_1) - 25y_{exp}(x_0)}{12\Delta h}$$

and similarly on the other side:

$$\frac{Flux(j)}{2p} = y'(1, \tau_j) = y'(x_N, \tau_j) \approx \dots$$

The errors are: $\frac{\Delta h^2}{6} y^{(3)}$, $\frac{\Delta h^4}{30} y^{(5)}$, $\frac{\Delta h^4}{5} y^{(5)}$.

Computing the flow or flux through the border $\partial\Omega$

To compute the diffusive flux $J(r, t)$, we use the **Fick's first law**

$$-D \nabla C(r, t) = J(r, t) \quad \text{on} \quad \partial\Omega \times [t_0, T].$$

Further, we use the term $Flux(j)$ for the total flux through the border, based on mass balance we have

$$Flux(j) = \frac{\partial}{\partial t} \int_{\Omega} C(r, t) dV.$$

In our 1D case, we compute for each j^{th} time instant

$$y_{sum}(j) = sstep \left[\frac{y_{exp}(x_0, \tau_j) + y_{exp}(x_N, \tau_j)}{2} + \sum_{i=1}^{N-1} y_{exp}(x_i, \tau_j) \right]$$

and set

$$Flux(j) = \frac{LC\{y_{sum}(j-2), y_{sum}(j-1), y_{sum}(j+1), y_{sum}(j+2)\}}{tstep}$$

where LC means 'a linear combination of' and

- **sstep** is a space step between two experimental data
- **tstep** is a time step between two experimental data

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Values p_j and $p_j(\alpha)$ are approximate solutions of minimization problems

$$p_j = \arg \min_p J_j(p), \quad p_j(\alpha) = \arg \min_p J_j(p, \alpha)$$

It holds

$$\lim_{\alpha \rightarrow 0} p_j(\alpha) = p_j$$

What we have for $\alpha \rightarrow \infty$:

- :-(solutions $p_j(\alpha)$ are more and more constant i.e. $p_j(\alpha) \equiv p_{reg} \quad \forall j$
- :-(function values $J_j(p_j(\alpha), \alpha)$ becomes larger (although there is a *supremum*).

We look for such a value α^* for which the relative standard deviation is 'small enough'.

Criterion called the **L-curve**:

We plot

- the value of objective function J (without the regularization term) against
- the average value $\bar{p}_j(\alpha)$ and the deviation of $p_j(\alpha)$ from $\bar{p}_j(\alpha)$ (or construct a combination when we know the exact solution p^*)

The L-curve optimal parameter α^* then corresponds to the point with maximal curvature.

For the plotting we use the following quantities:

1 Objective function J

$$J(p_1(\alpha) \dots p_M(\alpha)) = \sum_{j=0}^M \sum_{i=0}^N [y_{exp}(x_i, \tau_j) - y_{sim}(x_i, \tau_j, p_j(\alpha))]^2$$

2 „Relative“ deviation from the average value
(so-called coefficient of variation)

$$\sigma = \frac{1}{M \bar{p}_j(\alpha)} \sqrt{\sum_{j=1}^M [p_j(\alpha) - \bar{p}_j(\alpha)]^2}$$

3 Relative deviation from the solution

$$\omega = \frac{|\bar{p}_j(\alpha) - p^*| + \sigma}{p^*}$$

The algorithm

For a fixed regularization parameter α we determine diffusion coefficients $p_1(\alpha) \dots p_M(\alpha)$ in the following way:

- 1 Choose initial expected value p_{reg} and stopping tolerance ε_{reg}
- 2 Compute $p_j(\alpha)$, $j = 1 \dots M$, by minimizing functions

$$J_j(p, \alpha) = \left\{ \sum_{i=0}^N [y_{exp}(x_i, \tau_j) - y_{sim}(x_i, \tau_j, p)]^2 + \alpha (p - p_{reg})^2 \right\}$$

- 3 Compute the average value

$$\bar{p}_j(\alpha) = \frac{p_1(\alpha) + \dots + p_M(\alpha)}{M}$$

- 4 If

$$|\bar{p}_j(\alpha) - p_{reg}| \leq \varepsilon_{reg},$$

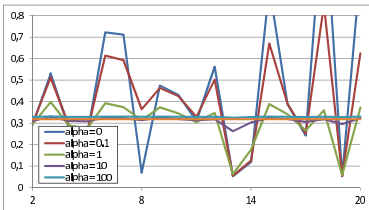
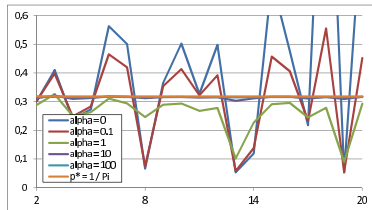
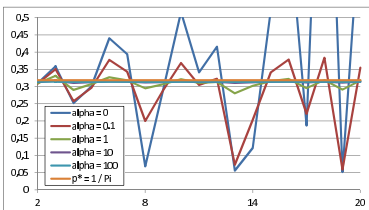
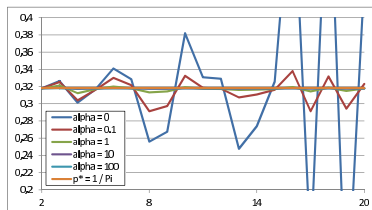
then STOP.

- 5 Set $p_{reg} = \bar{p}_j(\alpha)$ and go back to step 2.

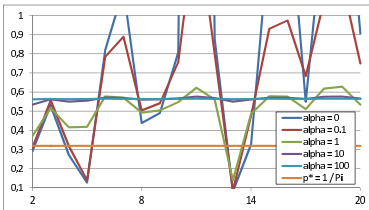
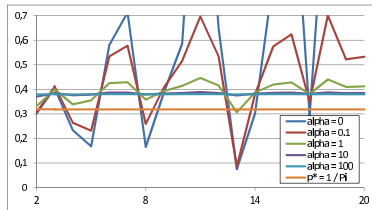
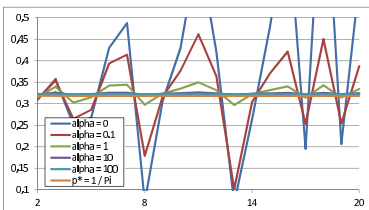
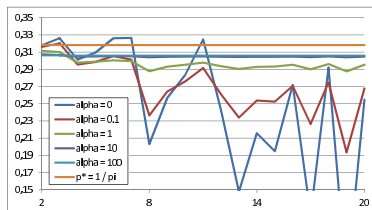
- 1 Introduction
- 2 1D diffusion-reaction equation
- 3 Single parameter estimation problem
- 4 Ill-posed problem
- 5 Implementation
- 6 Regularization
- 7 Numerical results**

Dirichlet boundary condition, noise = 1%, 5%, 10%, 20%:

j^{th} time instant against values p_j for different α



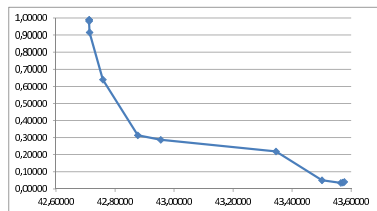
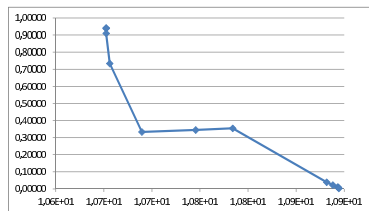
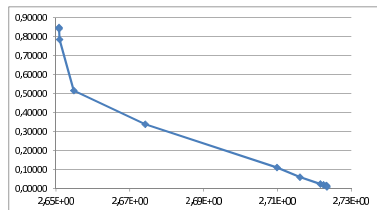
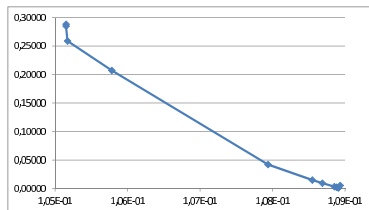
Neumann boundary condition, noise = 1%, 5%, 10%, 20%:
 j^{th} time instant against values p_j for different α



Dirichlet boundary condition, noise = 1%, 5%, 10%, 20%:

L-curve – values J against values ω

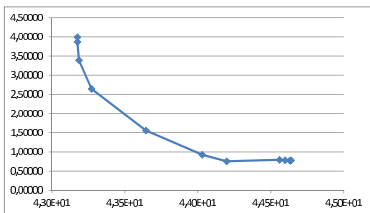
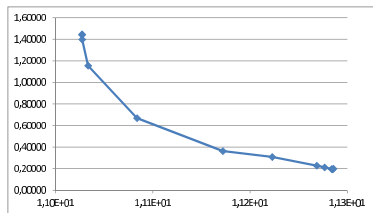
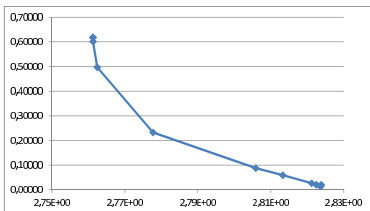
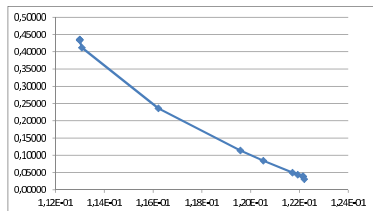
$\alpha = 0, 1d-4, 1d-3, 1d-2, 1d-1, 5d-1, 1, 5, 10, 50, 100, 500$



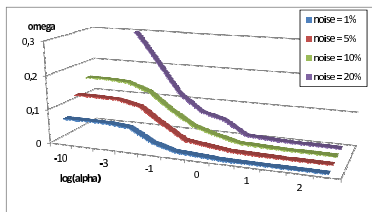
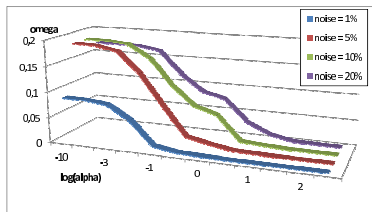
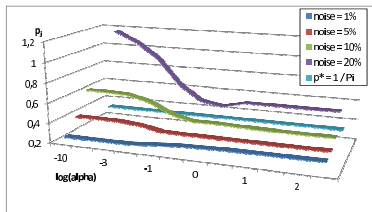
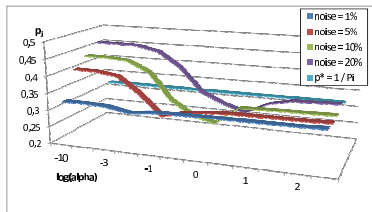
Neumann boundary condition, noise = 1%, 5%, 10%, 20%:

L-curve – values J against values ω

$\alpha = 0, 1d-4, 1d-3, 1d-2, 1d-1, 5d-1, 1, 5, 10, 50, 100, 500$



Values p_j for Dirichlet (UL) and Neumann (UR) boundary conditions;
 values of *deviation* for Dirichlet (BL) and Neumann (BR) b.c.



- Our method improves on other models by accounting for experimentally measured post-bleaching fluorescence profiles (i.e. not only the maximum depth point as CWM does) and time-dependent boundary conditions, and can include also a reaction term to account for the low level bleaching during scanning and the time varying fluorescence signal as well.
- Finding an optimal solution p is not a simple least square minimization problem. Due to the ill-posedness and noisy data it is quite a difficult task. We have already implemented a suitable regularization technique and a robust optimization procedure. In the near future we would like to improve our method by an adequate assessment of the measurement noise.
- For the previously known diffusion coefficient and the synthetic data simulated by the random walk model our program computes correct results. We determined the diffusivities for the real data of FRAP measurements (with the red algae *Porphyridium cruentum*). The range of result $10^{-14}\text{m}^2\text{s}^{-1}$ is in agreement with reference values.

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Mathematical and Computer Modelling (accepted)
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